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Title: Robust Reservoir Generation by Correlation-Based Learning

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Abstract

Reservoir computing (RC) is a new framework for neural computation. A reservoir is usually a recurrent neural network with fixed random connections. In this article, we propose an RC model in which the connections in the reservoir are modifiable. Specifically, we consider correlation-based learning (CBL), which modifies the connection weight between a given pair of neurons according to the correlation in their activities. We demonstrate that CBL enables the reservoir to reproduce almost the same spatiotemporal activity patterns in response to an identical input stimulus in the presence of noise. This result suggests that CBL enhances the robustness in the generation of the spatiotemporal activity pattern against noise in input signals. We apply our RC model to trace eyeblink conditioning. The reservoir bridged the gap of an interstimulus interval between the conditioned and unconditioned stimuli, and a readout neuron was able to learn and express the timed conditioned response.

1 Introduction

Liquid state machines (LSM)[1] and echo state networks (ESN)[2] are an emerging new framework for neural computation. They were proposed independently, and now are unified under the name of reservoir computing (RC)[3]. An RC model consists of a recurrent network called a “reservoir” that maps input signals into a higher dimension, and a set of neurons called “readouts” that receive inputs from the reservoir to extract time-varying information. The computational power of RC is outstanding[4], despite the simplicity of its structure and learning algorithm compared with conventional recurrent networks.

In the standard RC, the reservoir is assumed to have fixed random connections, although synaptic weights in the brain can change dynamically depending on internal states and external inputs. In this study, we consider the change of the computational performance of an RC model that possesses

learnability in its reservoir. Specifically, we apply correlation-based learning (CBL), which has widely been assumed in self-organizing neural systems[5, 6], to synaptic weights in the reservoir to examine whether the computational performance of the RC model is improved.

The reservoir generates a spatiotemporal activity pattern of neurons in response to an input stimulus, and reproduce the same spatiotemporal activity pattern when the same stimulus is given in the noise-free condition. If noise is added to the input stimulus, however, the generated activity pattern may change for the repetition of trials. We demonstrate that CBL modifies connection weights in the reservoir under the repeated presentations of input stimuli so that the model becomes to generate almost the same spatiotemporal activity patterns even in the noisy situation. This result suggests that CBL enables computational performance of the RC model to be noise-tolerant.

We also conduct the simulation of trace eyeblink conditioning[7] to demonstrate the performance of our RC model. In trace eyeblink conditioning, a subject is exposed to paired presentation of a transient conditioned stimulus (CS, e.g., brief tone) and an unconditioned stimulus (US, e.g., airpuff to the eye) that induces an eyelid closure with a temporal gap. After conditioning by repeated CS-US presentation, the subject learns to close its eye in response to the transient CS with a delay equal to the interstimulus interval (ISI) between the CS and US onsets (conditioned response; CR). In this conditioning paradigm, how to bridge the gap is an important issue. We demonstrate that our RC model bridges the gap by sustained activation of the reservoir and learns the CS-US association.

2 Materials and Methods

2.1 Model description

Figure 1 illustrates the schematic of our network model. The model is built on the basis of our previous model [8]. We added a new feature that synaptic weights between excitatory neurons are updated

according to CBL. The calculation of neural activity patterns and the update of synaptic weights are repeated several times, which we call trials. The model consists of N excitatory neurons and the same number of inhibitory neurons. Let $z_{\xi i}^{(k)}(t)$ be the activity of neuron i of type ξ at time t at trial k . $\xi \in \{\text{ex, inh}\}$ indicates either excitatory or inhibitory neuron type. Using $u_{\xi i}^{(k)}(t)$, which represents the internal state of the neuron, $z_{\xi i}^{(k)}(t)$ is defined as

$$z_{\xi i}^{(k)}(t) = \begin{cases} u_{\xi i}^{(k)}(t) & u_{\xi i}^{(k)}(t) > \theta_{\xi}, \\ 0 & \text{otherwise,} \end{cases} \quad (1)$$

where θ_{ξ} is the constant threshold. The dynamics of the internal states are given by the following equations:

$$\tau_{\text{ex}} \frac{du_{\text{exi}}^{(k)}}{dt} = -u_{\text{exi}}^{(k)}(t) + I_i^{(k)}(t) + \sum_j w_{\text{exi} \leftarrow \text{exj}}^{(k)} z_{\text{exj}}^{(k)}(t) - \sum_j w_{\text{exi} \leftarrow \text{inhj}} z_{\text{inhj}}^{(k)}(t), \quad (2)$$

$$\tau_{\text{inh}} \frac{du_{\text{inhi}}^{(k)}}{dt} = -u_{\text{inhi}}^{(k)}(t) + \sum_j w_{\text{inhi} \leftarrow \text{exj}} z_{\text{exj}}^{(k)}(t) - \sum_j w_{\text{inhi} \leftarrow \text{inhj}} z_{\text{inhj}}^{(k)}(t) \quad (3)$$

where τ_{ξ} is the time constant, $I_i^{(k)}(t)$ is the external input to excitatory neuron i at time t at trial k . A uniform noise with intensity η ($[-\eta, \eta]$) was added to $I_i^{(k)}(t)$ at each time step and for each neuron. $w_{\xi i \leftarrow \xi' j}$ is the weight of the synaptic connection from neuron j of type ξ' to neuron i of type ξ , where $\xi, \xi' \in \{\text{ex, inh}\}$. Synaptic weights among excitatory neurons are updated after every trial based on CBL as follows: for $k \geq 1$,

$$w_{\text{exi} \leftarrow \text{exj}}^{(k)} = \frac{\alpha}{\tau_w} \frac{\sum_{t=0}^T z_{\text{exi}}^{(k-1)}(t) z_{\text{exj}}^{(k-1)}(t)}{\sqrt{\sum_{t=0}^T (z_{\text{exi}}^{(k-1)}(t))^2} \sqrt{\sum_{t=0}^T (z_{\text{exj}}^{(k-1)}(t))^2}} + \left(1 - \frac{1}{\tau_w}\right) w_{\text{exi} \leftarrow \text{exj}}^{(k-1)}, \quad (4)$$

where $w_{\text{exi} \leftarrow \text{exj}}^{(0)}$ is set at $c_{\text{ex} \leftarrow \text{ex}}/N$ for any i and j , and $c_{\text{ex} \leftarrow \text{ex}}$ is a constant denoting the initial connection weight. The first term of the right-hand side in Eq. (4) represents the correlation between activities of excitatory neurons i and j , where T is the total simulation step for one trial, α is a constant scaling factor because the correlation takes the value between 0 and 1. The second term represents

a memory effect of excitatory synaptic weights over trials with a decay constant τ_w . We assume that $w_{\text{exi} \leftarrow \text{exi}}^{(k)} = 0$ for any k and i , indicating the absence of self-excitatory connections. $w_{\text{inhi} \leftarrow \text{exi}}$ is given under the binomial distribution $P(w_{\text{inhi} \leftarrow \text{exi}} = 0) = P(w_{\text{inhi} \leftarrow \text{exi}} = c_{\text{inh} \leftarrow \text{ex}}/N) = 0.5$. $w_{\text{exi} \leftarrow \text{inhi}}$ is set at $c_{\text{ex} \leftarrow \text{inh}}$ if $i = j$ and 0 otherwise: each inhibitory neuron inhibits its corresponding excitatory neuron. $w_{\text{inhi} \leftarrow \text{inhi}}$ is set at $c_{\text{inh} \leftarrow \text{inh}}/N$ for any i and j for simplicity, indicating all-to-all inhibition.

We defined two stimuli CS1 and CS2 fed into the network as follows:

$$\begin{aligned} \text{CS1 } I_i(t) &= \begin{cases} 1 & i \in \{0, \dots, 200\}, t \in \{0, \dots, 50\} \\ 0 & \text{otherwise,} \end{cases} \\ \text{CS2 } I_i(t) &= \begin{cases} 1 & i \in \{200, \dots, 400\}, t \in \{0, \dots, 50\} \\ 0 & \text{otherwise.} \end{cases} \end{aligned} \quad (5)$$

It should be noted that CS1 and CS2 activate different excitatory neurons in the reservoir.

2.2 Data analysis

We study how the activity pattern of excitatory neurons in the reservoir is evolved by the trigger of an input stimulus. To do this, first we define the autocorrelation of activities of excitatory neuron population at times t and $t + \Delta t$ at trial k as follows:

$$C^{(k)}(t, t + \Delta t) = \frac{\sum_i z_{\text{exi}}^{(k)}(t) z_{\text{exi}}^{(k)}(t + \Delta t)}{\sqrt{\sum_i (z_{\text{exi}}^{(k)}(t))^2} \sqrt{\sum_i (z_{\text{exi}}^{(k)}(t + \Delta t))^2}}. \quad (6)$$

The numerator represents the inner product of two populations of active excitatory neurons at times t and $t + \Delta t$, and the denominator normalizes the autocorrelation so that it falls in the range of $[0, 1]$ because $z_i^{(k)}(t)$ takes only positive values. It takes a value of 1 if these populations are identical, and it becomes 0 if no neurons are active at both times. We then define the similarity index at trial k by:

$$S^{(k)}(\Delta t) = \frac{1}{T} \sum_{t=0}^T C^{(k)}(t, t + \Delta t). \quad (7)$$

The similarity index is the average of Eq. (6) with respect to t . That is, this index represents how two populations separated by Δt are correlated, on average. In particular, it holds $S^{(k)}(0) = 1$ for any k because of trivial identity. It holds $S^{(k)}(\Delta t) = 0.5$ for some Δt , if the population of active excitatory reservoir neurons changes with time, and two populations separated by Δt are uncorrelated. It holds $S^{(k)}(\Delta t) = 0$ for some Δt , if any two populations separated by Δt have no overlap. Moreover, if the generation of the population of active excitatory reservoir neurons is nonrecurrent, the index would decrease monotonically. We define the standard deviation of the similarity index as well:

$$\sigma_S^{(k)}(\Delta t) = \sqrt{\frac{1}{T} \sum_{t=0}^T (C^{(k)}(t, t + \Delta t) - S^{(k)}(\Delta t))^2}. \quad (8)$$

We also define the reproducibility index at trial k as follows:

$$R^{(k)}(t) = \frac{\sum_i z_{\text{exi}}^{(k)}(t) z_{\text{exi}}^{(k-1)}(t)}{\sqrt{\sum_i (z_{\text{exi}}^{(k)}(t))^2} \sqrt{\sum_i (z_{\text{exi}}^{(k-1)}(t))^2}}. \quad (9)$$

The reproducibility index represents how two activity patterns of neurons at two successive trials are similar to each other at the identical time steps. If two activity patterns are completely identical, the index would be 1 for any t . If two activity patterns gradually diverge with time, the index gradually decreases.

The values of basic parameters are as the same as that we used previously [8] except $c_{\text{ex} \leftarrow \text{ex}}$. They are, $N = 1000, T = 3000, \tau_{\text{ex}} = 50.0, \tau_{\text{inh}} = 70.0, \theta_{\text{ex}} = 0.1, \theta_{\text{inh}} = 0.1, c_{\text{ex} \leftarrow \text{ex}} = 2.0, \alpha = 0.002, c_{\text{inh} \leftarrow \text{ex}} = 4.0, c_{\text{ex} \leftarrow \text{inh}} = 16.0, c_{\text{inh} \leftarrow \text{inh}} = 6.0$, and $\tau_w = 10$.

2.3 Simulation of trace eyeblink conditioning

We carry out simulation of trace eyeblink conditioning to demonstrate the performance of our RC model.

We consider a simple model which has one readout neuron. The neuron is fed the output of all excitatory neurons in the reservoir through modifiable connections. The activity of the readout neuron

$o(t)$ is given by:

$$o(t) = \sum_{i=1}^N w_i z_{\text{exi}}(t), \quad (10)$$

where w_i is the connection weight from neuron i in the reservoir to the readout neuron. The readout neuron receives the binary instruction signal $e(t)$ as well. The connection weights are updated at each time step as follows:

$$w_i(t) = w_i(t) + \begin{cases} 1 & z_{\text{exi}}(t) > 0 \text{ and } e(t) = 1, \\ -0.002 & z_{\text{exi}}(t) > 0 \text{ and } e(t) = 0, \\ 0 & \text{otherwise} \end{cases} \quad (11)$$

This rule represents that the connection from a neuron is strengthened if the neuron is active and the instruction is given simultaneously, and that the connection is weaken if the neuron is active but the instruction is not given. In other words, conjunctive stimulation of the afferent and instruction inputs makes the connection stronger, whereas stimulation of only the afferent input weaker.

We use CS1 and CS2 as CSs, and define 2 USs (US1, US2) as follows:

$$\begin{aligned} \text{US1 } e(t) &= \begin{cases} 1 & t = 300 \\ 0 & \text{otherwise,} \end{cases} \\ \text{US2 } e(t) &= \begin{cases} 1 & t = 1000 \\ 0 & \text{otherwise,} \end{cases} \end{aligned} \quad (12)$$

CSs and USs are paired and presented to the network as described below.

3 Results

3.1 Generation of a sequence of active neuron populations

First, we studied the basic property of our reservoir. Figure 2a represents the activity pattern of the

first 100 out of N excitatory neurons ($z_{\text{exi}}(t) > 0$) when the network received CS1. These neurons became active immediately after the stimulus onset, and underwent random repetition of transitions between active and inactive states for $t > 50$. The random repetition of state transitions was sustained even after the cessation of the input stimulus at $t = 200$, which is due to the recurrent connections among excitatory neurons. Thus, the transient input stimulus evoked the sustained neural activity. Different neurons exhibited different temporal transition patterns, and so the population of active neurons changed gradually with time. This random transition of neural activity was made by the random recurrent inhibitory connections between excitatory and inhibitory neurons. The connections projected a population of active neurons into another, uncorrelated population of active neurons repeatedly, and the nonrecurrent sequence of populations of active neurons was generated. To confirm the nonrecurrence of this sequence, we calculated its similarity index in Fig. 2b. The index takes 1 at $\Delta t = 0$ because of the trivial identity. The index monotonically decreased as Δt deviated from 0, indicating that two populations of active neurons temporally separated by Δt became dissimilar as Δt increased. Taken together, our reservoir generated a nonrecurrent sequence of populations of active excitatory neurons by the trigger of a transient input stimulus. Because there is one-to-one correspondence between a time step from the stimulus onset and one population of active neurons at the time, the sequence of active neuron populations can represent the passage-of-time from the stimulus onset.

We then examined the robustness of the sequence generation against noise in input signals. We ran two simulations with different noise and calculated the reproducibility index between the two sequences of active neuron populations. As shown in Fig. 2c, the reproducibility was highest at $t = 0$ and monotonically decreased towards 0.85 as time elapsed, suggesting that these two sequences were almost identical at first, and then they diverged into different sequences gradually with time. This decrease ended at $t = 1000$ and after that the reproducibility index was almost constant (data not shown), suggesting that although we conducted simulation for 3000 time steps ($T = 3000$), the present model

was capable of representing only the first 1000 time steps under the current parameter setting. In the following, therefore, we showed simulation results only for the first 1000 time steps. We also calculated the reproducibility index between the activity pattern generated in response to CS1 and a random activity pattern to obtain a lower bound of the index. As the random activity pattern, we used the activity pattern generated in response to CS2. We found that the index quickly increased from 0 to 0.8 within 500 time steps, and was kept constant thereafter (data not shown). Therefore, the reproducibility index with a random activity pattern is lower than 0.85 in the steady state.

Some other properties, including how to stop the sustained neural activity, has been reported previously [8].

3.2 Enhanced robustness of CBL in sequence generation

Next, to examine the effect of CBL on the robustness in sequence generation, we carried out 21 simulations repeatedly with CS1 as an input stimulus. We calculated 20 reproducibility indices for 20 pairs of two successive trials and 20 similarity indices for 20 single trials.

Figure 3 represents similarity (a) and reproducibility (b) indices at 1st, 10th and 20th trials. The similarity did not change largely across trials, whereas the reproducibility increased trial by trial. This result indicates that CBL makes the sequence generation robust, without affecting the nonrecurrence property.

3.3 Embedding two sequences in a single reservoir

Reservoirs have ability to map different inputs into different spatiotemporal activity patterns in a higher dimension [9, 10]. We questioned whether our reservoir has the same ability, and conducted the following simulation. Figure 4a shows the schematic of instructive presentation of 2 CSs to the reservoir. We repeated 10 sets of trials of CS presentation. Each set of trials consists of a pair of CS1 trials

followed by another pair of CS2 trials. For each set of trials, we calculated the reproducibility indices for responses to CS1 and CS2 using a pair of CS1 trials and that of CS2 trials, respectively.

Figure 4b shows these reproducibility indices. Here, RI1, RI2, RI3, and RI4 denote the indices for CS1 and CS2 at the first trial and the indices at the final trial, respectively. Compared between RI1 and RI3, and RI2 and RI4, the reproducibility of responses to CS1 and CS2 was evidently increased at the 10th set of trials. This result suggests that CBL enhanced the robustness of the sequence generation for 2 different stimuli simultaneously.

3.4 Simulation of trace eyeblink conditioning

We carried out two simulations of trace eyeblink conditioning. In the first simulation, CS1 was paired with both US1 and US2 to examine whether our RC model can learn multiple timings. In the second simulation, CS1 was paired with US1, whereas CS2 with US2. By this simulation, we studied whether two sequences generated by CS1 and CS2 represent different memory traces.

Figure 5a shows the readout activities when CS1 was paired with both US1 and US2 with or without CBL. In both cases with or without CBL, the first peak appeared clearly at $t \approx 300$. The building-up activity started at $t \approx 600$ and reached the maximum at $t = 1000$ (data not shown). Namely, there is the second peak at $t = 1000$. The width of the second peak was larger than that of the first peak, suggesting that the precision of representation of longer time becomes worse. On the other hand, CBL improved the reproducibility of the activity pattern generation in the reservoir by strengthen connections between correlated neurons while weaken between less-correlated neurons. This manipulation increased the overall activity of the reservoir and made the output signal to the readout stronger. As a result, the amplitude of the readout activity became larger with CBL than without CBL.

Figure 5b shows activities of the readout neuron after the separate conditioning of CS1-US1 and CS2-US2. The activity of the readout neuron in response to CS1 reached the maximum around $t =$

300, and then gradually decreased. On the contrary, the readout activity in response to CS2 steadily increased and reached the maximum at $t = 1000$. Both cases showed single peak activities around the instructed times, indicating that there was little crosstalk between two sequences of active neuron populations for CS1 and CS2. Thus, our reservoir with CBL has potency to generate distinct sequences of active neuron populations for different input stimuli.

4 Discussion

In conventional RC, a reservoir is composed of neurons interconnected with fixed connection weights, and acts as a static nonlinear filter that maps input signals into a higher dimension. Because the dynamics is deterministic due to the fixed connections, a reservoir generates the identical output signals for the identical input stimulus in noise-free condition. In noisy condition, however, the reservoir could generate different output signals for the identical input stimulus. To generate the almost identical output signals despite the presence of noise, learning must be incorporated. In this article, we parsimoniously extended the convention of RC so that the synaptic weights between excitatory neurons are allowed to change according to CBL. The CBL improved the reproducibility of the output signals for the identical input stimulus in the noisy condition. This made the output signals to readout neurons stronger, and eventually increased the amplitude of readout neurons. Therefore, CBL was demonstrated to be useful for robust RC against noise. We also conducted the simulation of trace eyeblink conditioning and confirmed that the readout neuron was able to learn and represent the instructed time.

In the construction of our reservoir, connections between excitatory neurons work to sustain neural activity even after the cessation of input stimuli, these between inhibitory neurons control the total activity of neurons, and recurrent random connections between excitatory and inhibitory neurons cause random repetition of transitions between active and inactive states of neural population. This con-

struction seems consistent with experimental studies, which suggest that inhibitory neurons play an important role for generating complex spatiotemporal activity patterns of excitatory neurons in the olfactory bulb during odour discrimination [11] and in the prefrontal cortex during working memory tasks [12]. Moreover, these functional roles of the connections in our RC model elucidate properties of the reservoir beyond a blackbox generating spatiotemporal activity patterns as in the previously proposed RC models [1, 2].

The present model can represent up to 1000 time steps under the current parameter setting. We could extend the maximal time steps by, for example, scaling the time constants (τ_{ex} , τ_{inh}). We could also reduce the inhibition to excitatory neurons $c_{\text{ex} \leftarrow \text{inh}}$ to increase the reproducibility index, which, however, increases the similarity index as well and results in the worse separation of two time steps in the simulation of trace eyeblink conditioning. There is a trade-off between increasing the reproducibility and decreasing the similarity.

Correlation-based learning incorporated in the reservoir modified the connections among excitatory neurons such that connections between well-correlated neurons are strengthened, whereas these between less-correlated neurons are weakened. Owing to CBL, the network was self-organized and the generation of sequence of active neuron populations became noise-tolerant. Furthermore, it would be of interest to examine the property of the resulting connection matrix after the learning in terms of, for example, sparseness or scale-freeness.

Although RC is a promising concept in the field of modern neural computation, many problems remain to be solved for enabling its practical use. One of the important problems was how to determine neural connections to achieve robust and efficient reservoirs. Incorporation of CBL that we showed here provides a simple solution to construct robust reservoirs automatically.

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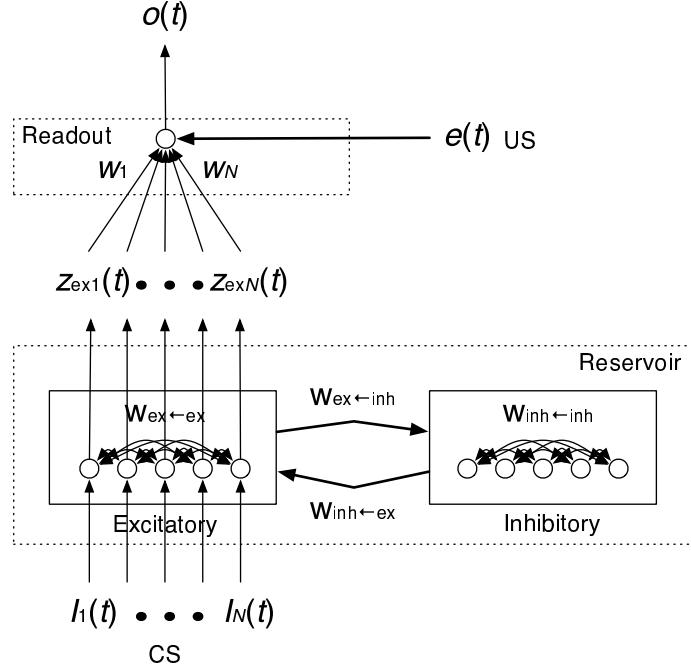


Figure 1: Schematic of our network model. The model consists of two networks: the reservoir and readouts. The reservoir is a recurrent network composed of excitatory and inhibitory neurons. Excitatory neurons receive external inputs representing conditioned stimuli (CS, Eq (5)). Four types of connections, excitatory to excitatory, excitatory to inhibitory, inhibitory to excitatory, and inhibitory to inhibitory, are assumed. Connection weights between excitatory neurons are modifiable by CBL (Eq. (4)), whereas the weights of other connections are fixed as in conventional RC models. On the other hand, a readout neuron receives inputs from excitatory reservoir neurons ($z_{exi}(t)$, $1 \leq i \leq N$) and the input representing unconditioned stimuli (US, Eq (12)). The connection weights between excitatory reservoir neurons and the readout neuron are modifiable by supervised learning rule (Eq. (11)).

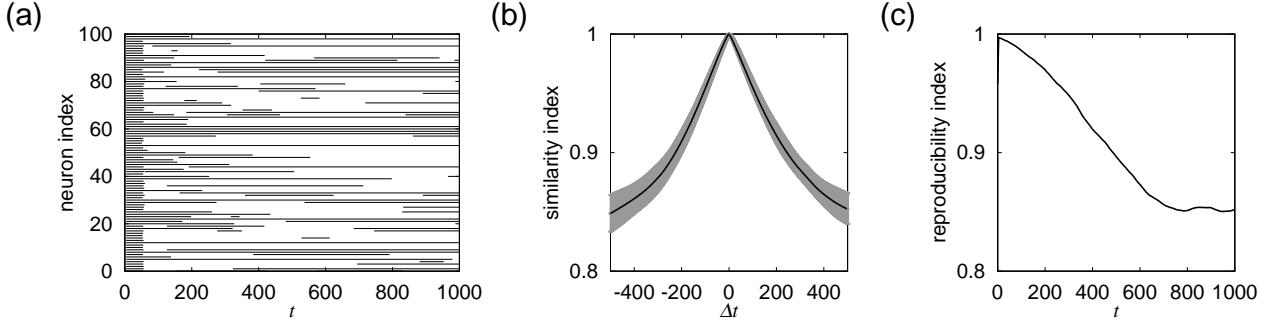


Figure 2: The basic property of the reservoir in our RC model. (a) Active states of the first 100 out of N excitatory neurons ($z_{\text{exi}}(t) > 0$). The abscissa and ordinate represent time and neuron index, respectively. A horizontal line represents the duration of the active state of a neuron. (b) The similarity index of this activity pattern. The abscissa and ordinate are time difference (Δt) and the index, respectively. The solid line indicates the mean index value, whereas the gray region represents the standard deviation of the index. (c) The reproducibility index between two sequences of active neuron populations generated under different noise. The abscissa and ordinate represent time and the index, respectively.

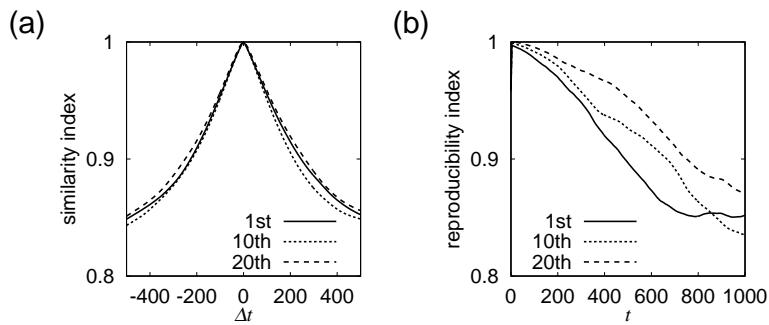


Figure 3: Effect of CBL for the sequence generation against noise. (a) Similarity indices for the sequences of active neuron populations at 1st (solid line), 10th (dotted line) and 20th (dashed line) trials. (b) Reproducibility indices for the same sequences at the same trials. Conventions as in Figs. 2b,c.

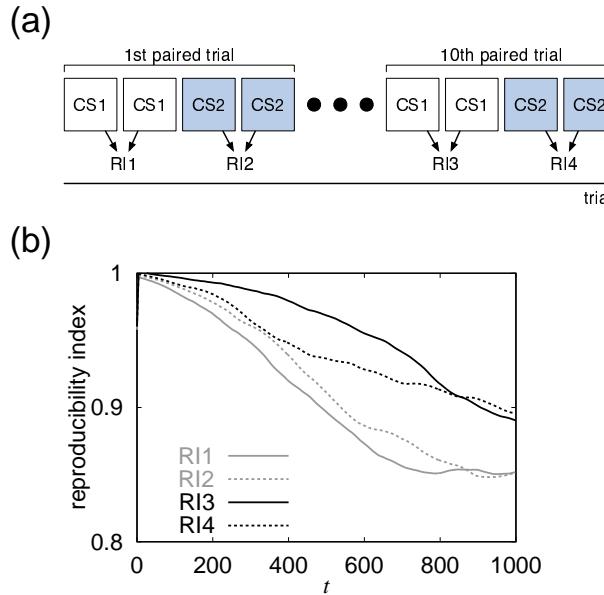


Figure 4: Embedding two sequences in a single reservoir. (a) Schematic of the simulation. Ten sets of trials of the simulation were conducted. Each set of trials consisted of a pair of CS1 trials and a successive pair of CS2 trials. Reproducibility indices between (1) CS1 trials at the 1st trial set, (2) CS2 trials at the 1st trial set, (3) CS1 trials at the last trial set, and (4) CS2 trials at the last trial set were calculated and labeled as RI1, RI2, RI3, and RI4, respectively. (b) Reproducibility indices obtained from simulations. RI1 (gray solid line), RI2 (gray dotted line), RI3 (black solid line) and RI4 (black dotted line) were plotted. Conventions as in Fig. 2c.

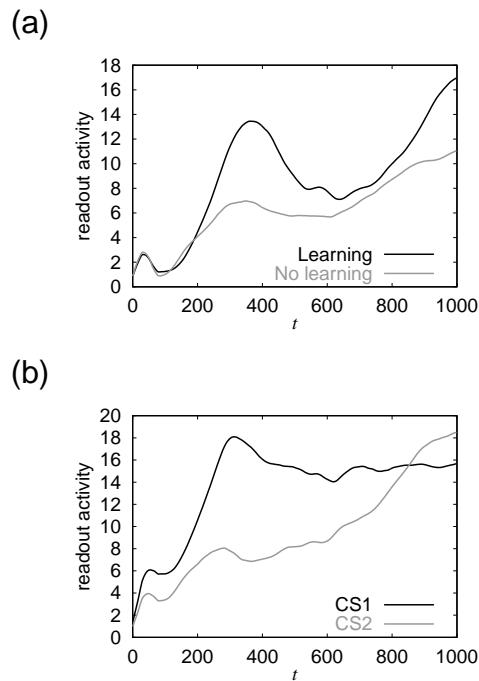


Figure 5: Activity of the readout neuron in the simulation of trace eyeblink conditioning. (a) Activities of the readout neuron with CBL (black line) and without CBL (gray line). The simulation was performed under the pairing of CS1 with both US1 ($t = 300$) and US2 ($t = 1000$). (b) Activities of the readout neuron when CS1 was paired with US1 (solid line) and when CS2 was paired with US2 (dotted line). The abscissa and ordinate represent time and the activity of the readout neuron, respectively.